

Numerical Simulation of Transport and Diffusion in Drainage Media

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Outline

- ▶ introduction, medical problem
- ▶ generate appropriate geometry
- ▶ advection through blood vessels
- ▶ diffusion in tissue
- ▶ coupling



Introduction

- ▶ RF ablation of tumors:
- ▶ numerical simulation of thermal processes
 - ▶ heat diffusion in tissue
 - ▶ transport of heat by blood flow through vessel system
 - ▶ develop tools in 2D to keep things simpler



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2D Vessel Trees

Geometric Structure

Flow Velocities

Advection Problem

Single Segments

ELLAM

Unknowns at Bifurcations

Basis and Test Functions at Bifurcations

Terminal Segments

Coupling to Diffusion Problem

Exchange of Energy

Heat Conduction in Tissue



Difference to 3D Case

3D vs 2D — what are the differences?

Blood vessels in 3D organs:

- ▶ can use “real” data obtained by medical imaging
- ▶ arterial and venous tree can “wind around each other”

In contrast, for 2D:

- ▶ no real-world data available for pairs of vessel trees
- ▶ need to generate appropriate system artificially
- ▶ individual segments have codimension 1



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Geometric Structure

- ▶ For simplicity: straight line segments & bifurcations
- ▶ Method by Schreiner et al. 1994 (for single tree): Constrained Constructive Optimization (CCO).
 - ▶ add nodes at random positions one-by-one
 - ▶ “optimize” connection to existing tree
- ▶ extended to pair of trees:
 - ▶ avoid mutual intersections
 - ▶ ensure minimum distance (in some sense)



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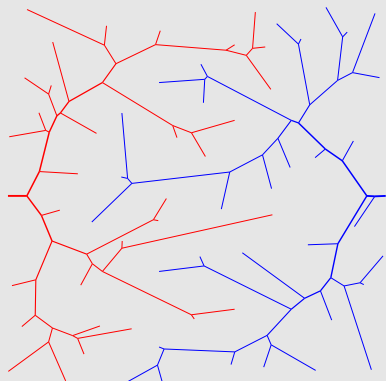
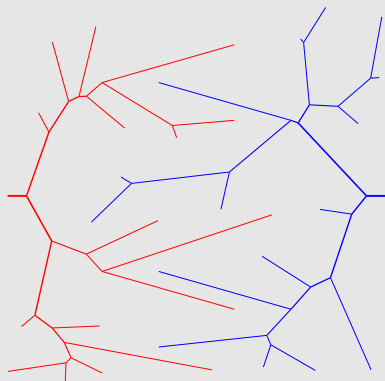


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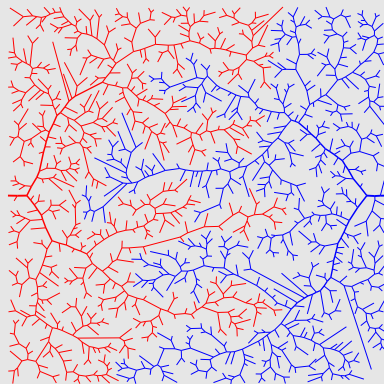
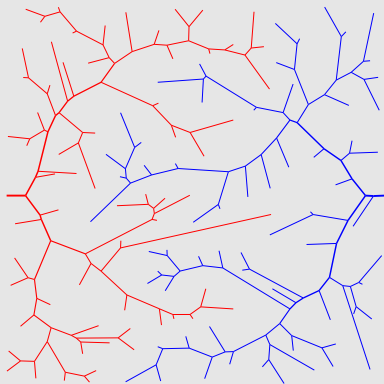
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Pairs of Vessel Trees (geometric structure)



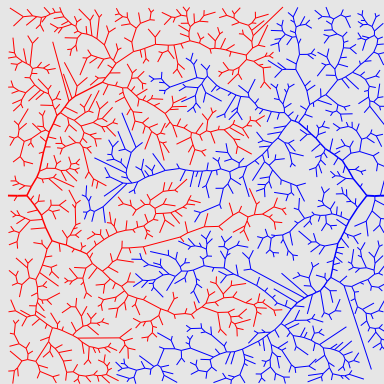
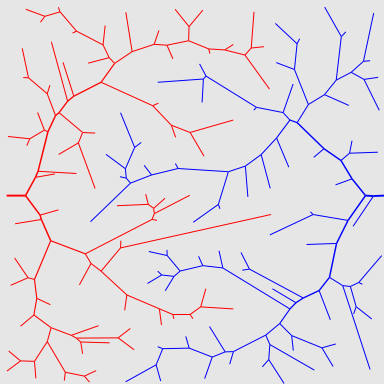
Pairs of Vessel Trees (geometric structure)



But what about flow velocities?



Pairs of Vessel Trees (geometric structure)



But what about flow velocities?



Flow Velocities

Balance flow velocities to avoid artificial wide-range components.

- ▶ Model: vector $S \in \mathbb{R}^{\approx 1000}$
 - ▶ outflow out of arterial terminal segments
 - ▶ inflow into venous terminal segments
 - ▶ both are assumed constant on each segment
 - ▶ mass conservation at bifurcations and in domain
- ▶ pressure p in domain depends on S via PDE
- ▶ minimize dissipation of kinetic energy by friction:
$$E(p) = \int_{\Omega} \nabla p \cdot \nabla p$$
- ▶ discretize and optimize subject to “nasty” constraints



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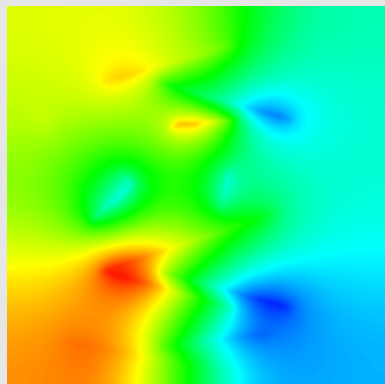
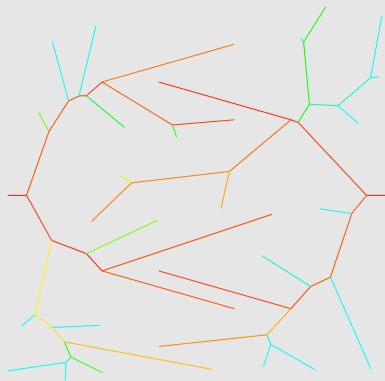
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Flow velocities and pressure profile



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Advection in Vessel Trees: Overview

- ▶ single segments
- ▶ \prec and \succ bifurcations
- ▶ terminal segments
- ▶ trees

1D Advection

First consider 1D advection with constant velocity:

$$\partial_t u(t, x) + v \partial_x u(t, x) = f(t, x) \quad (1)$$

$u(t, x)$ is energy content (energy per length = energy density times cross section area).

To solve initial-boundary value problem numerically, use ELLAM (Eulerian-Lagrangian Locally Adjoint Method) by Celia et al. (1990)



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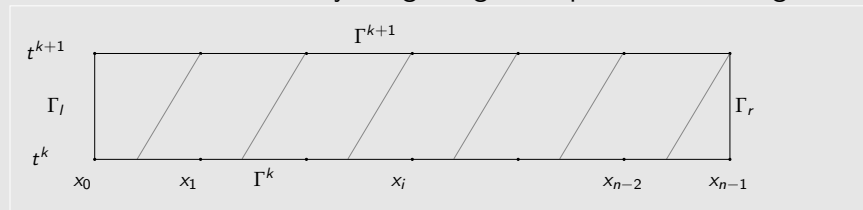
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Obtain weak formulation by integrating over space-time rectangle

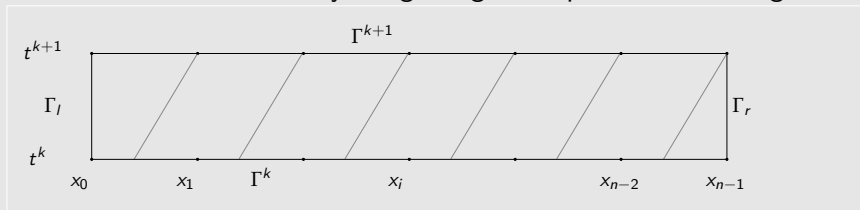


$$\int_0^\ell \int_{t^k}^{t^{k+1}} (\partial_t + v \cdot \partial_x) u \cdot w = \int_0^\ell \int_{t^k}^{t^{k+1}} f \cdot w \quad (2)$$

ELLAM: for test functions w constant along characteristic curves.



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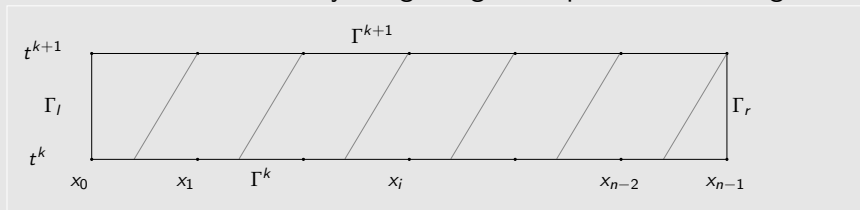


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Integrate by parts in space and time:

$$\begin{aligned}
 & \int_{\Gamma^{k+1}} u(t^{k+1}, x) \cdot w(t^{k+1}, x) \, dx - \int_{\Gamma^k} u(t^k, x) \cdot w(t^k, x) \, dx \\
 & + \int_0^\ell \int_{t^k}^{t^{k+1}} u(t, x) \underbrace{(-\partial_t - v \cdot \partial_x) w(t, x)}_{=0 \text{ (ELLAM test function)}} \, dt \, dx \quad (3) \\
 & + v \cdot \int_{\Gamma_r} u(t, \ell) w(t, \ell) \, dt - v \cdot \int_{\Gamma_l} u(t, 0) w(t, 0) \, dt \\
 & = \int_0^\ell \int_{t^k}^{t^{k+1}} f(t, x) \cdot w(t, x) \, dx \, dt
 \end{aligned}$$



Discretization

Basis functions:

- ▶ Nodal basis functions: piecewise linear hat functions,
 - ▶ height = cross section area of segment
 - ▶ discrete values are proportional to temperature

Test functions:

- ▶ At “new” time level: same shape as basis function,
- ▶ height = 1 (partition of unity)
- ▶ constant along characteristic curves
- ▶ roof-shaped in space-time

Restriction for time step: $v \leq 1 \frac{\text{grid cell}}{\text{time step}}$



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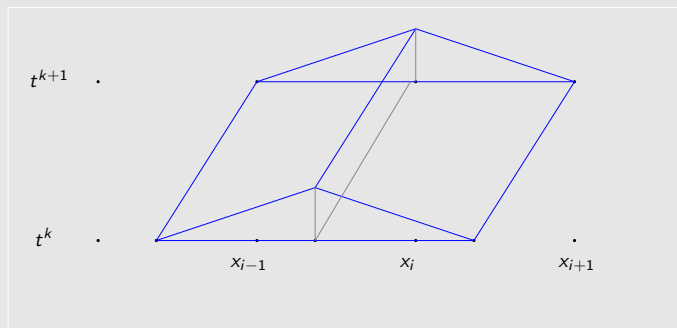
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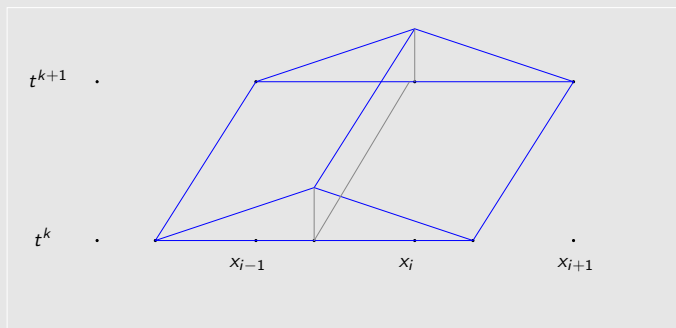
Test Functions



Evaluate products of base functions and test functions.



Test Functions

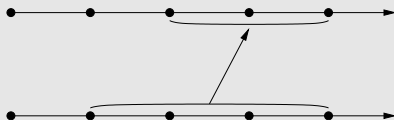


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ELLAM

which leads to a scheme:



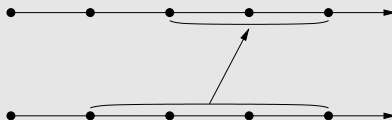
$$\begin{bmatrix} * & * & & & \\ * & * & * & & \\ & * & * & * & \\ & & \ddots & \ddots & \ddots \\ & & & * & * & * \\ & & & & * & * \end{bmatrix} \begin{bmatrix} \vdots \\ \vdots \\ n \\ e \\ w \\ \vdots \\ \vdots \end{bmatrix} = \begin{bmatrix} * & * & & & \\ * & * & * & & \\ * & * & * & * & \\ & \ddots & \ddots & \ddots & \ddots \\ & & * & * & * & * \\ & & & * & * & * \end{bmatrix} \begin{bmatrix} \vdots \\ \vdots \\ o \\ l \\ d \\ \vdots \\ \vdots \end{bmatrix}$$

Gaußian elimination?



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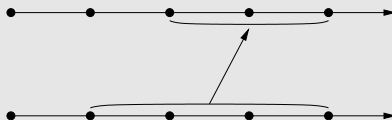


$$\begin{bmatrix}
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Gaußian elimination?

Arterial Bifurcations

- ▶ Flow is split $\frac{A_d v_d}{A_p v_p} : \frac{A_e v_e}{A_p v_p}$.
- ▶ Temperature is split continuously
- ▶ temperature content is split $\frac{A_d}{A_p} : \frac{A_e}{A_p}$.



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Venous Bifurcations

- ▶ Flow is combined $\frac{A_d v_d}{A_p v_p} + \frac{A_e v_e}{A_p v_p}$.
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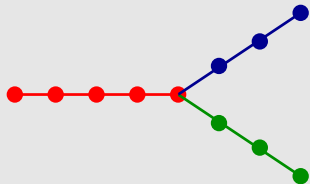


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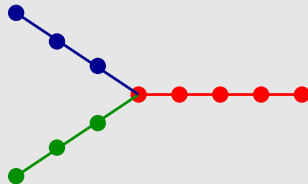
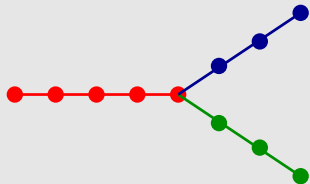
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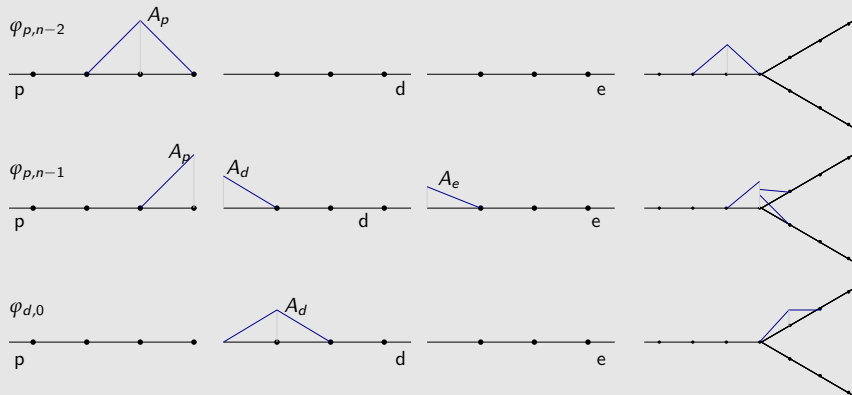
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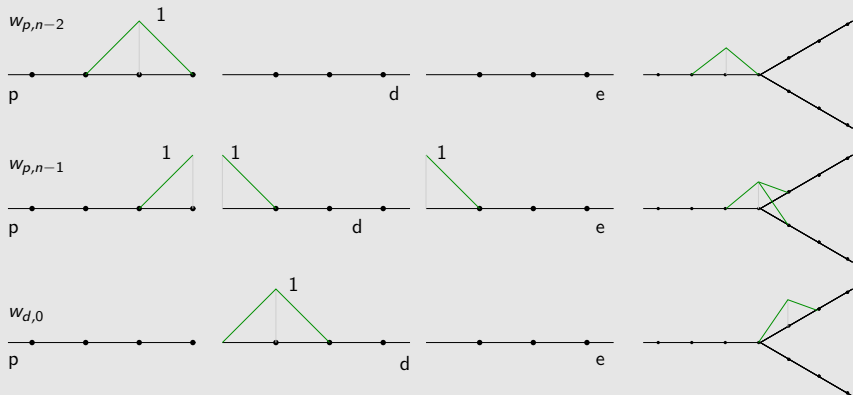
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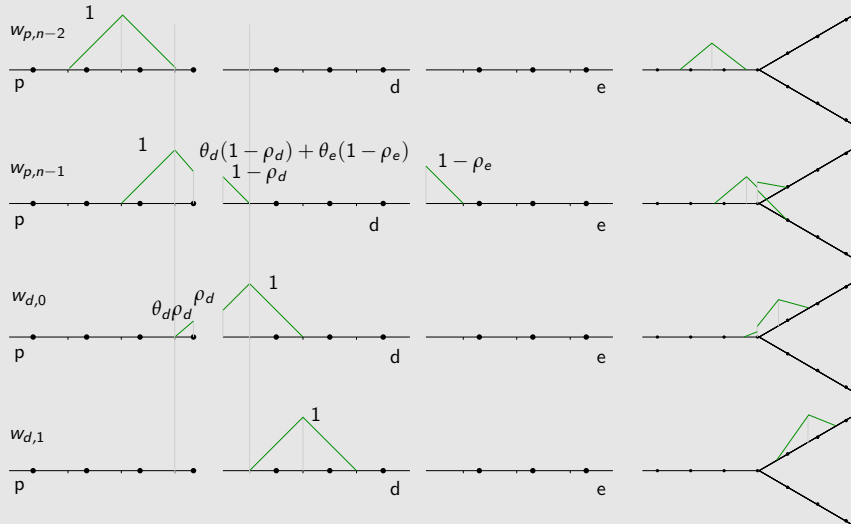
Basis Functions at Arterial Bifurcations



Test Functions at Arterial Bifurcations



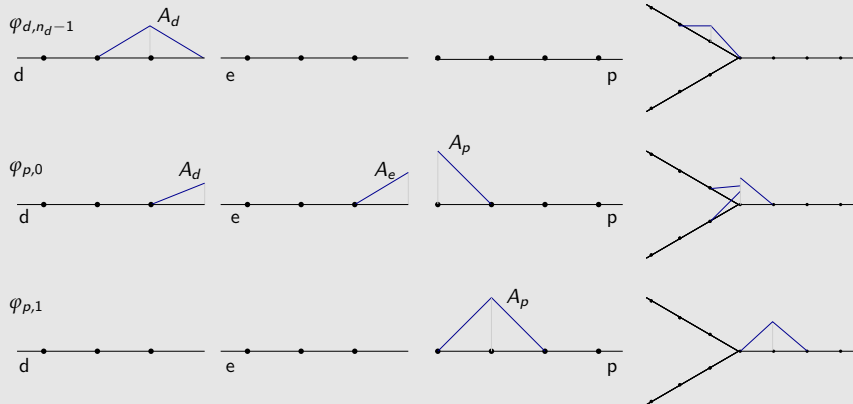
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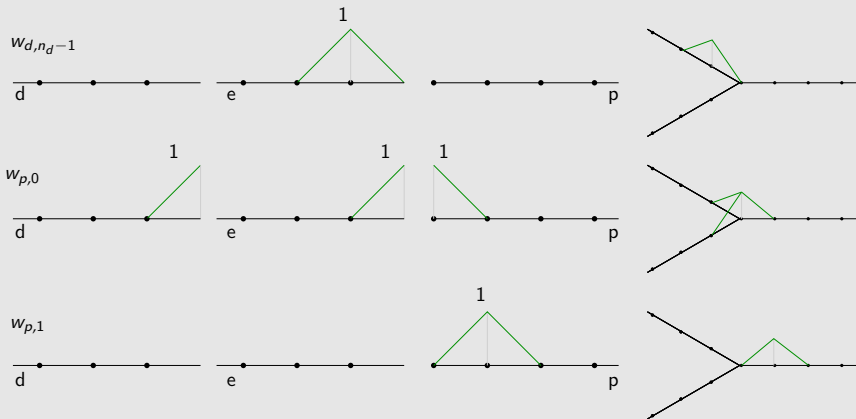
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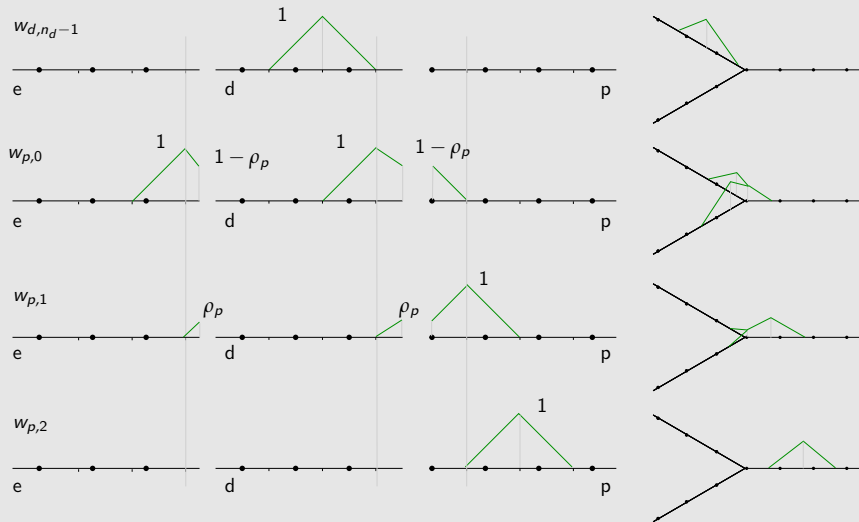
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Corresponding System of Equations

- ▶ one “big” system of equations
- ▶ block structure
 - ▶ diagonal blocks almost as before
 - ▶ coupling between segments $\hat{=}$ off-diagonal blocks (very few entries)
 - ▶ sparse, but no longer banded system (Gaußian elimination not efficient)
 - ▶ use conjugate gradient solver (no preconditioning)



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Advection at \prec bifurcation

movie: splitting of a temperature profile



Advection at γ bifurcation

movie: continuous combination of temperature profiles



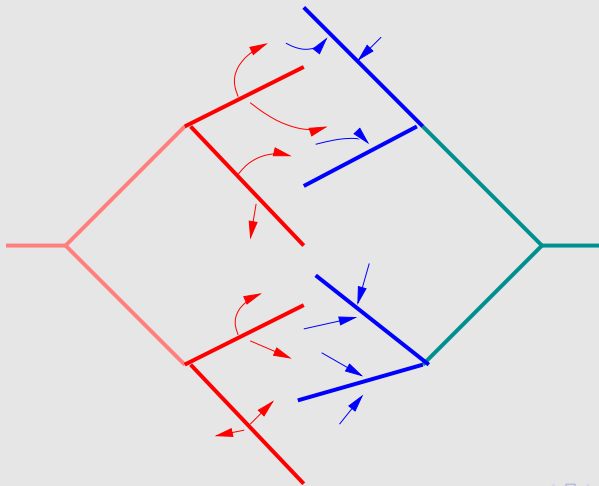
Advection at γ bifurcation

movie: discontinuous combination of temperature profiles



Terminal Segments

- ▶ Outflow of mass out of arterial terminal segments (and only these)
- ▶ Inflow of mass into venous terminal segments (and only these)



Arterial Terminal Segments

- ▶ Constant inflow temperature \Rightarrow constant temperature throughout segment
- ▶ linear drop-off of temperature content towards end point (3D: quadratic?)

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- ▶ could use bigger time step
 - ▶ may need to trace back through multiple bifurcations
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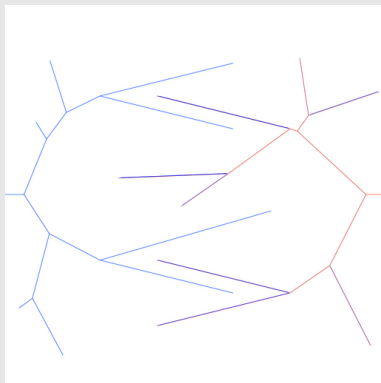


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Advection: Results



Outline

2D Vessel Trees

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Terminal Segments

Coupling to Diffusion Problem

Exchange of Energy

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Coupling to Diffusion Problem

Want to model RF ablation in tissue with blood flowing through vessels.

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 - ▶ (RF probe) source in tissue to
 - ▶ advection problem through vessel systems
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First idea: Mass carries energy, so use source terms proportional to mass flow

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Better: Microscopic view.

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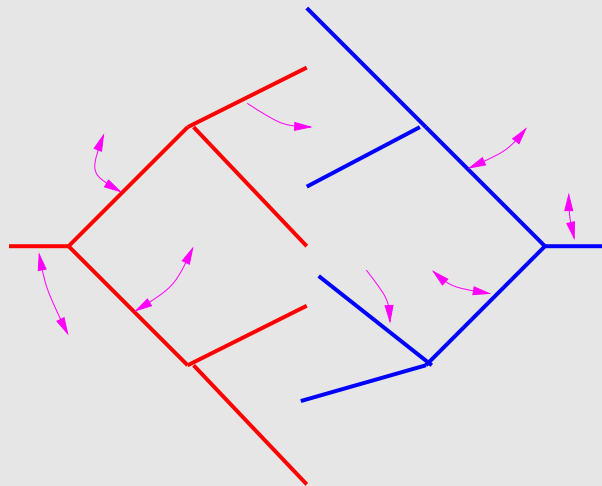
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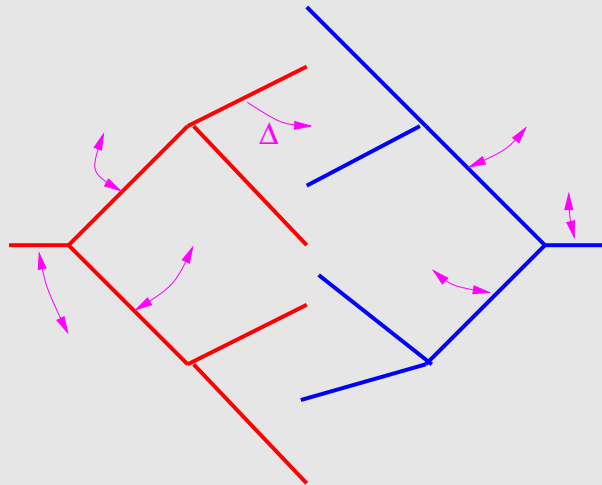
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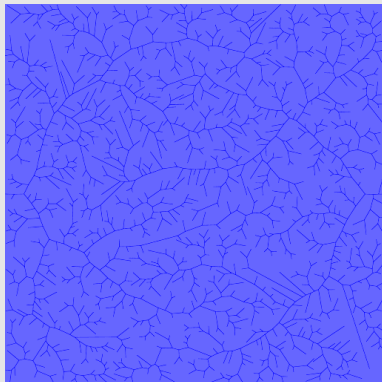
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Pulses of Inflowing Warm Blood

Artificial problem: Inflowing pulses of warm blood, pulsed flow velocities.

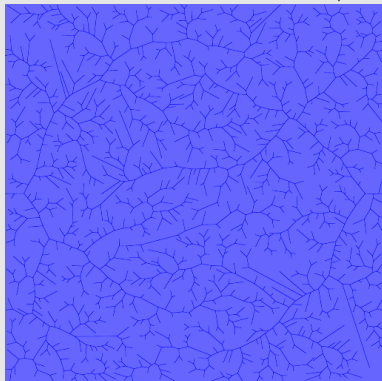
Different color scales for tissue / vessel temperature.



Pulses of Inflowing Warm Blood

Now place RF probe near arterial vessel.

Same color scale for tissue / vessel up to opacity.



Outlook

► 3D

- more complicated geometric structure
- diffusion within vessels
- advection within tissue
- more detailed model of physical effects (vessel walls, non-laminar flow within vessels, thermal influence of RF probe)
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References

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