MODELING FLOW THROUGH REALISTIC, ALGORITHMICALLY GENERATED VASCULAR STRUCTURES IN THE LIVER

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The Liver

 central metabolic organ (glucose storage, detoxication, ...)





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- blood: organism ↔ liver by three vascular systems
 - hepatic artery (HA) supplies oxygen
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- ~ 1.5 M lobuli (∅ ≈ 1 mm) as functional units







Goal



- blood flow simulation (distribution of e.g. drug or contrast agent)
- using geometrically realistic model





Outline

1. Introduction

- 2. Constrained Constructive Optimization
- 3. Generating Realistic Vascular Systems
- 4. Application: Flow Simulations





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Cooperation Partners within Virtual Liver Network (funded by BMBF)

Niko Komin, Andrea Schenk (MEVIS) Uta Dahmen, Olaf Dirsch (UK Jena) Felix Gremse, Fabian Kiessling (UK Aachen) Markus Krauss, Lars Küpfer (BTS Leverkusen)





1. Introduction Contents

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Image Data Acquisition

- in vivo 3D imaging
- corrosion casts and µCT (3D)







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insufficient resolution for lobular scale





Generating Vascular Systems





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- 1. obtain geometric representation of real vascular tree structures (~150 clinical CT scans)
- 2. implement algorithm for generating vascular trees





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- 3. perform geometric analysis, evaluate measures of similarity
- 4. starting from coarsened trees, validate semi-fine generated against measured trees (validation/postprocessing)
- 5. starting from measured trees, generate additional resolution (application)







2. Constrained Constructive Optimization Contents

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2. Constrained Constructive Optimization Idea of the Algorithm

[Schreiner et al. 1993]

- find optimal vascular network for supplying/draining given volume
- assume homogeneous supply
- respect coarse anatomic details and organ shape
- physiologically reasonable assumptions, no angiogenesis model





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Input

- initial tree





2. Constrained Constructive Optimization Physical Assumptions

[Schreiner et al. 1993]

Edge radii determined by

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$$r_0^{\gamma} = r_1^{\gamma} + r_2^{\gamma}$$
 with $\gamma = 3$ (Murray's law)







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• r_1 and r_2 such that flow resistances of subtrees are balanced



Poiseuille's law for laminar flow

$$R = \frac{8 \cdot \text{viscosity} \cdot \text{length}}{\pi \cdot \text{radius}^4}$$





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- decreasing viscosity for radius < 150 µm (Fåhræus-Lindqvist effect)
- serial and parallel connection of edges (Kirchhoff's law)





Physiological Formulation

[Schreiner et al. 1993]

minimize

over





2. Constrained Constructive Optimization Physiological Formulation

[Schreiner et al. 1993]

minimize intravascular volume

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Physiological Formulation

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minimize intravascular volume + penalty for nodes outside liver

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minimize intravascular volume + penalty for nodes outside liver

over set of vascular trees (topology and geometry)

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over set of vascular trees (topology and geometry) with constant root radius supplying given leaf nodes with given outflow amounts





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Mathematical Formulation

[Schreiner et al. 1993]



Objective function for adding one leaf node

$$F(e, p_{split}) := Vol(T_{prev} \oplus (p_{leaf}; e, p_{split}))$$

- extended vascular tree with valid radii (as above)
- obtained from tree T_{prev}
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- by splitting edge $e \in \mathbb{N}_{\# \text{ edges in } T_{\text{prev}}}$
- at point $p_{\text{split}} \in \mathbb{R}^3$
- penalty term if p_{split} outside organ Λ





$$\tilde{F}_{e}(p_{split}) := \operatorname{Vol}\left(T_{prev} \oplus (p_{leaf}; e, p_{split})\right) + C \operatorname{dist}^{2}(p_{split}, \Lambda)$$

minimized by gradient descent with Armijo step size control.





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- no analytic derivative wrt. position of bifurcation







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Computationally expensive

- bifurcation moved ⇒ need to recompute 3 lengths and many radii
- no analytic derivative wrt. position of bifurcation
- not clear where (topologically) to introduce new bifurcation (e)







Implementation

[S. and Preusser 2012]

Multi"scale" procedure

- 40 candidate edges with closest midpoints
- 'rough' stopping criterion to select 20 candidates
- 'fine' stopping criterion to find best topology
- simple parallelization (OpenMP) possible





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Still $O(N^2 \log N)$ workload for N leaf nodes.





two vascular systems ⇐ disjoint set of leaf nodes, independent CCO





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Overview

[S. and Preusser 2012]

Goal

- analyze geometric features in real vascular systems
- check whether algorithm produces similar ones
- improve algorithm

Input

~ 160 human in vivo scans







cf. [Strahler 1957]

Rather than bifurcation orders, consider Strahler-type scheme







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[S. and Preusser 2012]

Geometric features at a single bifurcation







[S. and Preusser 2012]

Geometric features at a single bifurcation



- evaluate histograms for all datasets per level and feature
- perform pairwise Kolmogorov-Smirnov test (p = 0.05) for similarity
- compute percentages and weighted average over Strahler* orders





CCO Postprocessing

[S. and Preusser 2012]



Postprocessing

- angles between daughters φ_a too small
 - \rightarrow shift in direction of bisector





CCO Postprocessing

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Observation

- real vascular trees differ slightly from CCO output
- postprocess rather than build into optimization-based construction





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4. Application: Flow Simulations

Transport in Vascular Systems



consider concentration in blood





4. Application: Flow Simulations

Transport in Vascular Systems



- consider concentration in blood
- transport only through vascular structures





4. Application: Flow Simulations

Transport in Vascular Systems



- consider concentration in blood
- transport only through vascular structures
- constant flow velocity per edge (essentially 1D)
- discretized using Eulerian-Lagrangian Locally Adjoint Method (ELLAM) [Celia et al. 1990]





4. Application: Flow Simulations First Results: Dynamic Flow



mouse CCO model (5000 leaves each)





4. Application: Flow Simulations First Results: Dynamic Flow



concentration profile color-coded





4. Application: Flow Simulations First Results: Dynamic Flow



concentration profile color-coded

 \rightarrow video




4. Application: Flow Simulations Outlook

Extend by

- porous medium model for extravascular space
- ⇒ 3D transport





4. Application: Flow Simulations Outlook

Extend by

- porous medium model for extravascular space
- ⇒ 3D transport
- multiple substances
- reaction term to model metabolization
- pharmacokinetics simulation





Summary

- CCO to generate vascular structures
- comparison to measurements, postprocessing
- application: blood flow simulation

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